

# pH-Dependence of Extrinsic and Intrinsic $H^+$ -Ion Mobility in the Rat Ventricular Myocyte, Investigated Using Flash Photolysis of a Caged- $H^+$ Compound

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**ABSTRACT** Passive  $H^+$ -ion mobility within eukaryotic cells is low, due to  $H^+$ -ion binding to cytoplasmic buffers. A localized intracellular acidosis can therefore persist for seconds or even minutes. Because  $H^+$ -ions modulate so many biological processes, spatial intracellular pH ( $pH_i$ )-regulation becomes important for coordinating cellular activity. We have investigated spatial  $pH_i$ -regulation in single and paired ventricular myocytes from rat heart by inducing a localized intracellular acid-load, while confocally imaging  $pH_i$  using the pH-fluorophore, carboxy-SNARF-1. We present a novel method for localizing the acid-load. This involves the intracellular photolytic uncaging of  $H^+$ -ions from a membrane-permeant acid-donor, 2-nitrobenzaldehyde. The subsequent spatial  $pH_i$ -changes are consistent with intracellular  $H^+$ -mobility and cell-to-cell  $H^+$ -permeability constants measured using more conventional acid-loading techniques. We use the method to investigate the effect of reducing  $pH_i$  on intrinsic (non- $CO_2/HCO_3^-$  buffer-dependent) and extrinsic ( $CO_2/HCO_3^-$  buffer-dependent) components of  $H_i^+$ -mobility. We find that although both components mediate spatial regulation of pH within the cell, their ability to do so declines sharply at low  $pH_i$ . Thus acidosis severely slows intracellular  $H^+$ -ion movement. This can result in spatial  $pH_i$  nonuniformity, particularly during the stimulation of sarcolemmal  $Na^+$ - $H^+$  exchange. Intracellular acidosis thus presents a window of vulnerability in the spatial coordination of cellular function.

## INTRODUCTION

Regulation of intracellular pH ( $pH_i$ ) is essential for the maintenance of normal cellular function. In the mammalian heart, modest displacements of  $pH_i$  from its resting level of 7.1–7.2 occur physiologically, for example during increases in cardiac workload (1,2) and during extracellular acid-base disturbances (3,4). Because of the high chemical reactivity of  $H^+$ -ions, notably with intracellular proteins, such displacements affect the electrical (5) and contractile (4, 6) behavior of the heart, and must eventually be corrected via regulatory processes. Larger displacements of  $pH_i$  occur during clinical disorders such as myocardial ischemia (7) where they induce severe contractile dysfunction (6,8) and arrhythmia (9).

The regulation of cardiac  $pH_i$  is achieved by means of ion transport proteins, which translocate  $H^+$ ,  $OH^-$ , and  $HCO_3^-$  ions across the sarcolemma. Their ability to regulate  $pH_i$  depends on adequate  $H^+$ -ion mobility within the cytoplasmic compartment.  $H^+$ -diffusion, however, is severely restricted because of high intracellular  $H^+$ -buffering ( $\sim 50,000$ , equivalent to an intracellular buffering capacity of  $\sim 50$  mM). Most of this buffering occurs at histidine residues on intracellular proteins that, because of their large size, exhibit low mobility. We have shown that adequate  $H^+$ -mobility within ventricular myocytes is furnished by a population of lower molecular weight diffusible buffers, such as the histidyl dipeptides acetylcarnosine, acetylanserine, and homocarno-

sine (10). These chaperone  $H^+$ -ions around the cell on a mobile buffer shuttle, thereby enabling the spatial regulation of  $pH_i$ . One important feature of the shuttle is that, although it distributes  $H^+$ -ions within the cell, it results in an effective  $H_i^+$ -mobility ( $D_{H^+}^{app}$ , the apparent  $H^+$ -diffusion coefficient) more than two orders of magnitude lower than in unbuffered solution (11). Another important feature is that, when  $pH_i$  decreases, many of the diffusible buffers approach saturation by  $H^+$ -ions, causing a further fall in  $H_i^+$ -mobility (12). Low  $H_i^+$ -mobility can result in significant spatial nonuniformity of cytoplasmic  $pH_i$ , particularly when large fluxes of acid occur across the sarcolemma (13).

In addition to intrinsic buffers such as histidyl dipeptides, the major extrinsic buffer system,  $CO_2/HCO_3^-$  (carbonic buffer), can also shuttle  $H^+$ -ions spatially within a cell, particularly when catalyzed endogenously by the enzyme, carbonic anhydrase (14–16). It is not known, however, if this component of the buffer-shuttle is modulated by changes of  $pH_i$  in a manner similar to that observed for the intrinsic shuttle. In this work we have therefore examined the relative roles of extrinsic and intrinsic buffer in setting  $H_i^+$ -mobility in the ventricular myocyte, over a range of  $pH_i$  values. This permits an assessment of their physiological importance in the spatial regulation of  $pH_i$ .

To assess  $H_i^+$ -mobility, a local rise of  $[H^+]_i$  is typically induced in one region of the cytoplasm and its spatial dissipation imaged confocally using an intracellular pH-fluorophore, such as carboxy-SNARF. Current methods for locally displacing  $pH_i$  include  $H^+$  loading from an acid-filled

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patch-pipette (11), and local microperfusion of extracellular membrane-permeant acidic molecules such as  $\text{CO}_2$  or acetic acid (17,18). Such approaches can be technically demanding and may not be suitable for all cell-types. We have therefore tested a novel method for introducing  $\text{H}^+$ -ions into a cell, by uncaging them from the membrane-permeant, proton-donor compound, 2-nitrobenzaldehyde (NBA), using ultraviolet (UV) flash-photolysis. Apart from a brief report for a neuronal preparation (19), this technique has not been applied previously in intact cells. In this work, we explore its potential in isolated ventricular myocytes. We assess the suitability of NBA for local and whole-cell intracellular proton uncaging, we estimate the photolytic efficiency of the process, and we gauge its usefulness for measuring  $\text{H}_i^+$ -mobility in single cells, and cell-to-cell  $\text{H}^+$ -permeability in cell-pairs. Having validated the technique, we then use it to elucidate the  $\text{pH}_i$ -sensitivity of  $\text{H}_i^+$ -shuttling via extrinsic and intrinsic buffer.

## METHODS

### Cell isolation

Cardiac myocytes were isolated from ~300 g Sprague-Dawley rats (killed by cervical dislocation in accordance with UK Home Office guidelines) using a combination of mechanical and enzymatic (0.24 mg/ml Blendzymes III, Roche, UK) dispersion (11,16,20). Cells were stored in DMEM culture medium (Sigma, UK) at room temperature.

### Solutions

HEPES-buffered normal Tyrode (NT) solution contained (in mM): NaCl (135), KCl (4.5), HEPES (20),  $\text{CaCl}_2$  (2),  $\text{MgCl}_2$  (1), glucose (10). Solution pH was adjusted to 7.4 using 4 M NaOH.  $\text{CO}_2$ /bicarbonate-buffered NT contained (in mM): NaCl (120), KCl (4.5),  $\text{NaHCO}_3$  (22),  $\text{CaCl}_2$  (2),  $\text{MgCl}_2$  (1), glucose (10). Solution pH was adjusted to 7.4 by continuously bubbling with 5%  $\text{CO}_2$ . Where indicated, 1 mM NBA (from 1 M stock dissolved in methanol) was included in solutions. In some experiments with coupled cell-pairs, 60  $\mu\text{M}$   $\alpha$ -glycyrrhetic acid ( $\alpha\text{GA}$ ) was included in superfusates to block gap junctional channels (20). In other experiments, the enzyme carbonic anhydrase was blocked with 100  $\mu\text{M}$  acetazolamide (ATZ). All chemicals were obtained from Sigma.

### Cell superfusion

Experiments were carried out in a 500- $\mu\text{l}$  Plexiglas flow-through chamber with the base made from a thin, glass coverslip. To facilitate cell adhesion, the coverslip was coated before each experiment with 100  $\mu\text{l}$  0.01% poly-L-lysine (Sigma). After washing away poly-L-lysine, 200  $\mu\text{l}$  of cells in culture medium were applied to the superfusion chamber, mixed with 1.5  $\mu\text{l}$  1.7 mM solution of an acetoxymethyl (AM) carboxy-SNARF pH-fluorophore (Molecular Probes, Eugene, OR) in DMSO. For experiments at alkaline or resting  $\text{pH}_i$ , carboxy-SNARF-1 was used ( $\text{pK} = 7.5$ ), whereas at lower  $\text{pH}_i$ , the recently developed analog, carboxy-SNARF-4F ( $\text{pK} = 6.4$ ), was preferred (21). The physicochemical properties of the two dyes (e.g., their membrane permeability, molecular mass and chemical structure) are very similar, differing only by the  $\text{pK}$  shift in their emission spectra. After 10 min of dye-loading in darkness, cells were continuously supplied with superfusate. When required, two platinum wires along the length of the chamber were used to field-stimulate the cells.

## Confocal $\text{pH}_i$ imaging

Cells were imaged using an inverted confocal microscope (TCS NT system on a DM IRBE microscope; Leica, Wetzlar, Germany) equipped with a  $\times 63$  plano-apochromat, water-immersion objective (NA 1.2) with UV correction. The carboxy-SNARF dyes were excited by the 514-nm line from an Argon laser, and fluorescence emission was measured at  $580 \pm 20$  nm and  $640 \pm 20$  nm (line scan speed = 400 Hz). The ratio of fluorescence intensity measured at the two wavelengths was converted to pH using calibration curves obtained in separate experiments (22).

## $\text{H}^+$ -uncaging from NBA

After loading with pH-fluorophore, the cells were then loaded with the  $\text{H}^+$ -donor compound by including 1 mM NBA in all superfusates. This is highly membrane-permeant, superfusion typically commencing a few minutes before an experiment. Cells loaded with 1 mM NBA for 1 min produced the same magnitude of acid-uncaging as cells loaded for  $>3$  min. When exposed to UV light-flashes at 351 nm from a 20-mW UV laser (Enterprise II Laser; Coherent, CA), NBA undergoes an intramolecular redox reaction (23) giving 2-nitrosobenzoic acid (Fig. 2 A). The  $\text{pK}$  of 2-nitrosobenzoic acid is  $\sim 2.2$  and so the product is fully dissociated in the physiological  $\text{pH}_i$  range. Despite photolysis, the intracellular concentration of NBA remained constant owing to continued passive entry from the superfusate. Without electronic zoom, the ROI exposed to UV light could be as large as  $150 \times 150$   $\mu\text{m}$  (entire field of view) or as small as  $5 \times 5$   $\mu\text{m}$  (the smallest sweep length). At a pixel resolution of  $256 \times 256$  and a line-scan speed of 400 Hz, the UV laser dwell-time per pixel was  $\sim 10$   $\mu\text{s}$ . UV light intensity could be reduced by neutral-density filters to obtain the desired magnitude of intracellular acid-load. Since high-energy laser exposure tends to damage cells, two consecutive UV flashes of lower intensity, separated by 0.95 s (a flash-event), were preferred over a single, higher intensity exposure.

The excitation protocol could be programmed to switch automatically between Argon laser for carboxy-SNARF excitation and acquisition of  $\text{pH}_i$  data, and UV laser for flash-photolysis. Due to time delays imposed by the changes in microscope optics, the shortest transition time between "acquisition mode" and "photolysis mode" was 3–4 s.

## Presetting starting $\text{pH}_i$

Superfusion with NT stabilizes  $\text{pH}_i$  at 7.1–7.2. In some experiments,  $\text{pH}_i$  was preset uniformly to different levels before starting an experiment. To manipulate starting  $\text{pH}_i$ , cells were prepulsed (24,25) with solutions containing ammonium chloride or sodium acetate (based on NT solutions, with an appropriate reduction in  $[\text{NaCl}]$  to keep overall osmolarity constant at  $\sim 310$  mOsm/kg). After the prepulse, cells were returned to NT solutions containing no weak base or weak acid, resulting in an intracellular acidosis or alkalosis, respectively. By varying the dose of acetate (40–80 mM) or ammonium (10–30 mM) and the duration of the prepulse (4–8 min), it was possible to attain any desired  $\text{pH}_i$  value in the range 6.2–7.8. To clamp the  $\text{pH}_i$  to the new displaced level, measures were taken to block sarcolemmal acid/base transport pharmacologically or by ion-substitution.  $\text{Na}^+/\text{H}^+$  exchange (NHE) was blocked by including 30  $\mu\text{M}$  cariporide (Aventis, Germany) in superfusates (26,27). In  $\text{CO}_2$ /bicarbonate-buffered superfusates,  $\text{Na}^+/\text{HCO}_3^-$  cotransport (NBC) was 90% blocked by 10  $\mu\text{M}$  S0859 (Aventis) (27); in  $\text{CO}_2$ -free solutions, NBC was not active. In  $\text{CO}_2$ /bicarbonate-buffered superfusates, acid-loading transporters ( $\text{Cl}^-/\text{HCO}_3^-$  exchange and  $\text{Cl}^-/\text{OH}^-$  exchange) were blocked by replacing extracellular chloride salts with an equivalent concentration of gluconate salts (with an appropriate rise in total added  $[\text{Ca}^{2+}]$  from 2 to 8.5 mM to account for the binding of  $\text{Ca}^{2+}$  to gluconate) (28). In  $\text{CO}_2$ -free solutions, sarcolemmal  $\text{H}^+$ -equivalent influx at high  $\text{pH}_i$  is mediated by  $\text{Cl}^-/\text{OH}^-$  exchange (CHE) (25). Because this is kinetically slow ( $<1$  mM/min), no inhibitory measures were taken in experiments that lasted up to 2 min.

## Offline data processing

The confocal system produces three stacks of images: a spatial fluorescence map of the cell at 580 nm, a spatial fluorescence map at 640 nm, and the transmission image of the cell. The transmission image is used to describe the cell geometry, whereas the ratio of the fluorescence at 580 nm and 640 nm (after background offsetting) gives a measure of pH<sub>i</sub>. Raw data were processed into [H<sup>+</sup>]<sub>i</sub> time courses, averaged within rectangular ROIs (typically 15–20 μm by 15–20 μm), aligned along the length of the cell (macro written in Scion Image; Scion).

For H<sup>+</sup>-loading experiments using serial H<sup>+</sup>-ion uncaging, the mean time course of rise of [H<sup>+</sup>]<sub>i</sub> in each ROI was fitted with an algorithm for two-dimensional H<sup>+</sup>-diffusion from a constant source (defined by the UV-flash area). For single cells (16), the diffusion equation was solved over a single reflective compartment, defined by the geometrical boundary of the cell. The fitting procedure was solved using the finite element method, assuming a single value for the apparent intracellular H<sup>+</sup>-diffusion coefficient ( $D_H^{app}$ ) (29). By varying the starting level of [H<sup>+</sup>]<sub>i</sub> (see above) and restricting each best-fit to a fall in cell-averaged pH<sub>i</sub> of <0.3 pH-units, it was possible to discern the pH<sub>i</sub>-dependence of  $D_H^{app}$ , as described in the Results section. The estimate of  $D_H^{app}$  was assigned to a pH<sub>i</sub> value equal to the cell-averaged pH<sub>i</sub> at the mid-point of acid-loading. Different values for starting [H<sup>+</sup>]<sub>i</sub> were spaced as closely as 0.05 pH-units.

For experiments where the relaxation of a longitudinal pH<sub>i</sub>-gradient was imaged after terminating the local acid-uncaging sequence, [H<sup>+</sup>]<sub>i</sub> data were fitted to a two-dimensional reflective compartment model with a nonuniform initial condition. The entire relaxation period was used for best-fitting, and the estimate of  $D_H^{app}$  was assigned to the cell-averaged pH<sub>i</sub> at the midtime of relaxation.

In the case where H<sup>+</sup>-uncaging was performed locally in a cell-pair, the two-dimensional diffusion equation was solved (20) over two reflective compartments, coupled across the junctional membrane by a passive permeation flux, described by an apparent permeability coefficient ( $P_H^{app}$ ). The boundary condition for this junctional membrane was:  $H^+ \text{-Flux}_{\text{cell1} \rightarrow 2} = P_H^{app} \times ([H^+]_{\text{cell2}} - [H^+]_{\text{cell1}})$ .

Statistical analysis of data was performed using Student's unpaired *t*-test or by one-factor analysis of variation. The level of significance was set to 5%. Data are presented as mean ± SE.

## Measurements of cell-shortening and intracellular Ca<sup>2+</sup>

Experiments were carried out on an epifluorescence set-up built on a Nikon Diaphot microscope (Nikon, UK). Rat myocytes were AM-loaded with 10 μM of the Ca<sup>2+</sup>-indicator, Fluo-3 (Molecular Probes). During superfusion

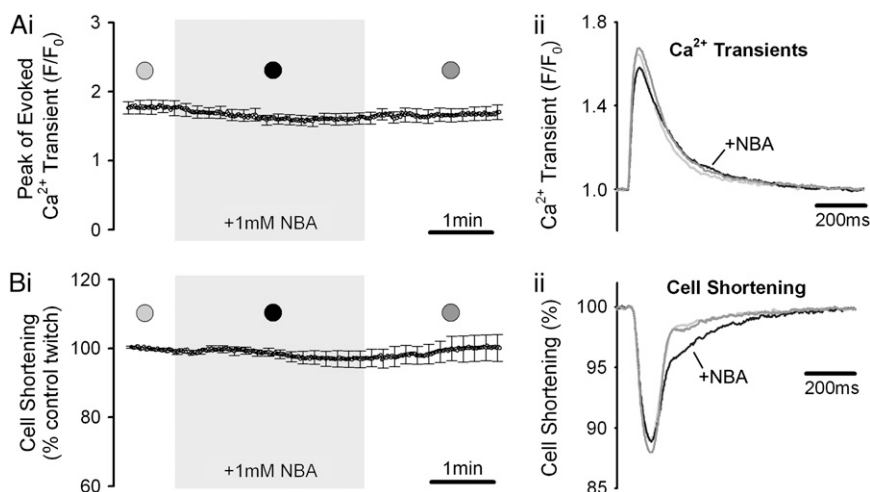
with HEPES-buffered NT, cells were electrically field-stimulated (60–70 V, 0.2-ms pulses at 1 Hz from an isolated DC stimulator). Intracellular fluorophore was excited by a Xenon lamp monochromator (Optoscan, Cairn, UK) at 488 nm and Ca<sup>2+</sup>-sensitive fluorescence >515 nm was measured with a photomultiplier tube. Cell contraction was measured simultaneously using an edge-detection device (Crescent Electronics, UT) that utilized the transmission image of the cell. Data were digitized with a CED 1401plus digitizer (Cambridge Electronic Design, UK) and recorded with Spike2 software (Cambridge Electronic Design). Ca<sup>2+</sup> data are presented as a ratio, relative to diastolic Ca<sup>2+</sup> ( $F/F_0$ ); cell-shortening has been normalized to the control value averaged over the first minute of stimulation.

## RESULTS

### Effect of 2-nitrobenzaldehyde on excitation-contraction coupling

Isolated myocytes were electrically activated by field stimulation at 1 Hz. Fig. 1, *Aii* and *Bii*, show simultaneous recordings of the evoked Ca<sup>2+</sup>-transient and cell-shortening before, during, and after a 3-min exposure to 1 mM NBA. The caged H<sup>+</sup>-compound did not affect the time course or amplitude of the Ca<sub>i</sub><sup>2+</sup>-transient (Fig. 1 *A*), and had no influence on peak cell-shortening (Fig. 1 *B*), indicating that it does not disrupt excitation-contraction coupling. In 5 out of 10 cells, however, a reversible slowing of the late phase of relaxation was observed. We did not investigate this phenomenon further as it was not a consistent occurrence, and there was no other detectable effect of NBA. The slowing was most likely due to direct interference of NBA with the myofilaments or the cell's viscoelastic machinery, rather than an influence on intracellular Ca<sup>2+</sup> dynamics, as relaxation of the Ca<sup>2+</sup>-transient was unaffected.

When superfused with 1 mM NBA (*n* = 10), myocytes typically remained quiescent and rod-shaped for at least 10 min, whereas, with 5 mM NBA (*n* = 10), cells usually survived for no more than 5 min. At 10 mM NBA, cells rapidly developed membrane blebs and displayed hypercontracture within 1–2 min. NBA was therefore applied at 1 mM in all subsequent experiments.



**FIGURE 1** Effect of 2-nitrobenzaldehyde on excitation-contraction coupling. Rat myocytes were superfused with HEPES-buffered media and field-stimulated at 1 Hz. After a period of pacing (>1 min), cells were exposed to superfusates containing 1 mM NBA. The evoked Ca<sup>2+</sup>-transient (*A*) and cell-shortening (*B*) were measured simultaneously (mean ± SE; *n* = 10). (*Ai*) Peak systolic Ca<sub>i</sub><sup>2+</sup>-fluorescence is plotted versus time (peak systolic,  $F$ , normalized to diastolic Ca<sup>2+</sup>-fluorescence,  $F_0$ ). (*Bi*) Mean contraction amplitude (for each experiment, normalized to initial control contraction [averaged over 1 min]) is plotted versus time. (*Aii*) Superimposed time courses of Ca<sup>2+</sup>-transients from a representative experiment, taken at times indicated in panel Ai. (*Bii*) Superimposed time courses of cell-shortening, taken from same experiment as *Aii*.

## Whole-cell flash-photolysis

When UV light is scanned across the entire area of a cell,  $\text{pH}_i$  should decrease uniformly, provided the intracellular concentration of NBA is uniform. This assumption is likely to hold true because NBA is a membrane-permeant, low molecular-weight solute (151 Da) that is neither charged nor subject to transmembrane transport or metabolism. NBA had no effect on resting  $\text{pH}_i$  until the cell was exposed to UV light (see Figs. 2 *B*, 4 *Ai*, 5 *Ai*, 6 *A*). Fig. 2 *B* shows data pooled from several experiments where the entire field of view encompassing a cell was exposed to UV flash-events at 0.11 Hz (indicated by the *arrows*), interposed by 2-s periods of  $\text{pH}_i$  data-acquisition (with 2-frame averaging). Photolytic redox of extracellular NBA did not lead to accumulation of extracellular acid because uncaged protons were washed away by continuous superfusion.  $\text{H}^+$ -ions uncaged within the cell, however, produced a cumulative fall of  $\text{pH}_i$  of  $\sim 0.65$   $\text{pH}_i$  units within 3.5 min at 50% laser intensity (*solid circles*). This acid-load was not extruded, as the cell was superfused with a  $\text{CO}_2/\text{HCO}_3^-$ -free solution (to inhibit NBC) containing 30  $\mu\text{M}$  cariporide (to inhibit NHE).

The change of  $\text{pH}_i$  ( $\Delta\text{pH}_i$ ) plotted for each flash-event in Fig. 2 *B*, when multiplied by an appropriate value of buffering capacity (16), reveals the quantum of acid uncaged ( $J_q$ ). Fig. 2 *C* plots  $J_q$  as a function of time, for the successive flash-events illustrated in Fig. 2 *B*.  $J_q$  is relatively constant, indicating that the quantum was independent of the level of  $\text{pH}_i$ . Note that the cumulative fall of  $\text{pH}_i$  plotted in Fig. 2 *B* is curved rather than linear, because  $\text{pH}$  is a logarithmic function of  $[\text{H}^+]$ , and intrinsic buffering capacity increases as  $\text{pH}_i$  falls (16,25). Thus, even though  $\text{H}^+$ -release per flash-event is constant, the resulting  $\Delta\text{pH}_i$  is increasingly attenuated as  $\text{pH}_i$  falls.

The magnitude of the cumulative acid-load depended on the intensity of UV light, which could be varied by means of neutral density filters. Halving the laser intensity from 50% to 25% (by introducing a higher neutral density filter) reduced the mean acid-loading rate during the flash-sequence (Fig. 2 *B*, *shaded circles*), and halved the quantum of acid released per event (Fig. 2 *C*).  $J_q$  could therefore be graded experimentally.

The amplitude and time course of  $\Delta\text{pH}_i$  during a flash-event is shown at higher resolution in Fig. 2 *D*. Here, rat myocytes were exposed to flash-events of different laser

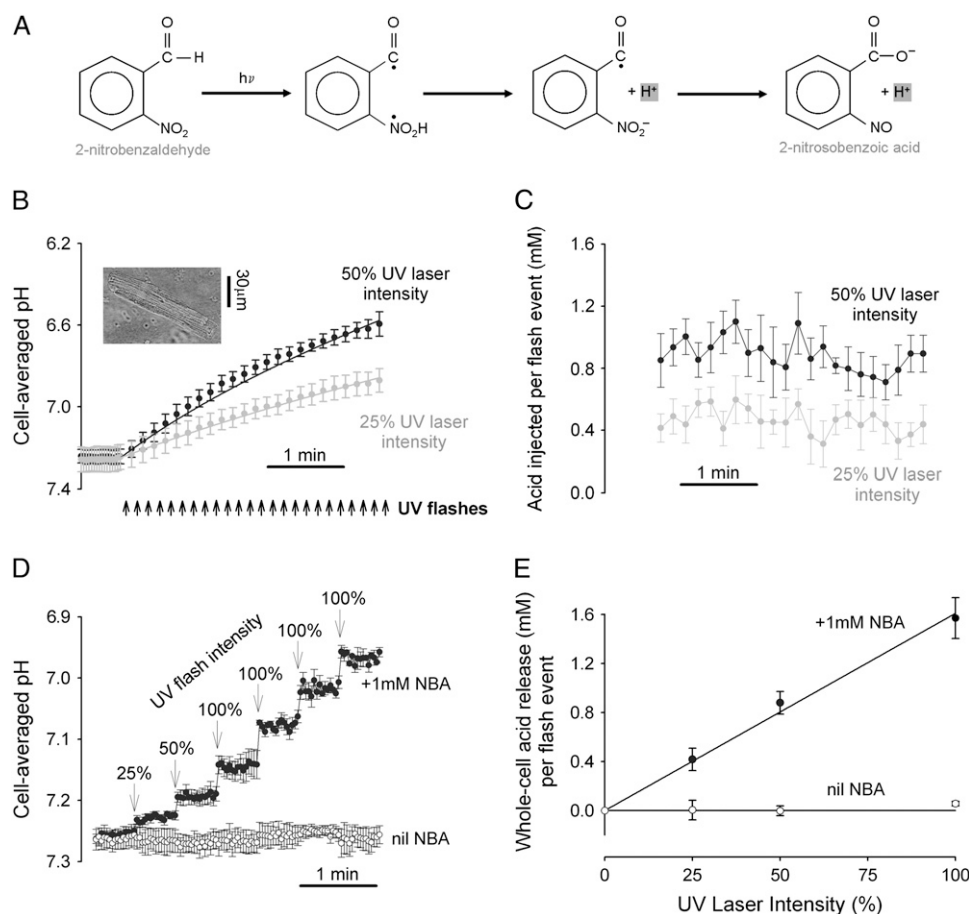


FIGURE 2  $\text{H}^+$ -uncaging in whole-cell (A). The energy from UV light catalyzes the intramolecular redox between the nitryl and aldehyde group of 2-nitrobenzaldehyde, producing 2-nitrosobenzoic acid which dissociates to its anion and  $\text{H}^+$ . (B) Inset shows rat myocyte superfused with HEPES-buffered NT containing 1mM NBA and 30  $\mu\text{M}$  cariporide. (Main panel) repetitive exposure of entire myocyte to UV flash events at 0.11Hz (denoted by arrows) produces a cumulative acidification which was monitored in between flash-events using carboxy-SNARF fluorescence: acid-loading rate, 4.16 mM/min at 25% laser intensity (*shaded circles*;  $n = 10$ ) and 8.14 mM/min at 50% laser intensity (*solid circles*;  $n = 10$ ). The continuous curves show model-predictions for constant acid-injection rates into a compartment with a buffering capacity as defined in (16). (C) The amount of acid released per flash-event, calculated from the change in  $\text{pH}_i$  after each flash-event multiplied by the intrinsic buffering capacity ( $n = 10$ ). (D) Rat myocytes were superfused with HEPES-buffered NT containing 30  $\mu\text{M}$  cariporide. In some experiments, 1 mM NBA was included in superfusates. Cells ( $n = 6$  with NBA,  $n = 7$  without NBA) were exposed to a UV flash-event of varying magnitude (25–100% of full power) every 30 s. Between flash events,  $\text{pH}_i$  was imaged every 2.1 s. (E) The stepwise fall in  $\text{pH}_i$  recorded in D was converted into a measure of acid released per flash-event ( $J_{\text{inj}} = -\Delta\text{pH} \times \beta$ ), using values for buffering-capacity ( $\beta$ ) measured previously (16). This has been plotted as a function of laser intensity. Data points in all panels shown as mean  $\pm$  SE.

intensity (once at 25%, once at 50%, and then four times at 100% intensity), each followed by a 30-s period of pH<sub>i</sub> data acquisition. The superfusates were again HEPES-buffered and contained 30 μM cariporide to inhibit sarcolemmal acid-extrusion. Each flash-event produced a rapid and sustained fall of pH<sub>i</sub>, (*solid circles*) whereas the whole sequence induced a series of stepwise decreases of pH<sub>i</sub>. The results therefore indicate that H<sup>+</sup>-uncaging is both rapid and irreversible. Because of the delay between UV-exposure and pH<sub>i</sub>-recording in our apparatus, we were unable to resolve the kinetics of uncaging but, in aqueous solution, it is known to occur within nanoseconds (30). Note that the flash sequence produced no change of pH<sub>i</sub> in the absence of NBA (*open circles*), indicating that the source of acid was indeed NBA redox. It also confirms that UV laser-light itself did not influence the fluorescent signal from the pH reporter-dye.

The constancy of pH<sub>i</sub> immediately after a flash-event indicates that acid release was uniform along the vertical axis of the cell, and also that the photolytic product, 2-nitrosobenzoic acid, does not flux significantly from the cell (if this happened, the acid-load would be dissipated). Fig. 2 *E* plots the mean quantum of H<sup>+</sup>-release as a function of laser intensity. This increases linearly with UV light intensity, reaching 1.6 mM acid released per event for 100% laser power. This represents a quantum yield for an individual UV flash of ~80% (1 flash-event = 2 individual flashes separated by 0.95 s; see Methods). The absence of saturation of acid-release with increasing laser power suggests that NBA photolyzed at the flash site is replenished rapidly i.e., sarcolemmal permeation of NBA is not a rate-limiting factor for intracellular H<sup>+</sup>-uncaging.

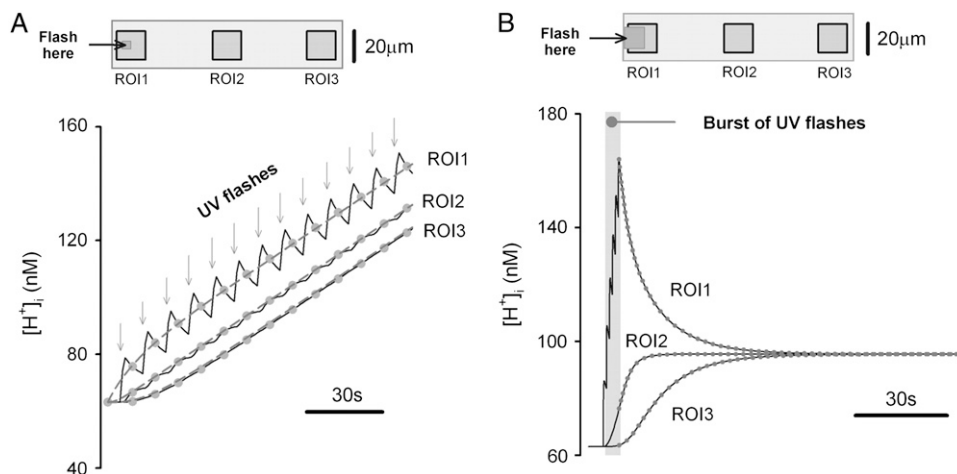
### Regional flash-photolysis: modeling H<sup>+</sup>-uncaging protocols

By confining the UV laser-scanning area to a small region of the cell, a local acidosis can be produced. This local pH<sub>i</sub>

change then drives dissipative H<sup>+</sup>-fluxes that obey Fickian diffusion. Two experimental protocols were used to drive these dissipative H<sup>+</sup>-fluxes: i), the H<sup>+</sup>-load was ramped up locally in a stepwise manner using a prolonged burst of identical flash-events, and the rise of H<sup>+</sup>-ion concentration in adjacent regions was monitored between flash-events; and ii), the local H<sup>+</sup>-load was established by a shorter rapid burst of flash-events, and its subsequent dissipation upon termination of the burst was monitored. The kinetics of the dissipative H<sup>+</sup>-fluxes, whether driven during or after the acid-load, were quantified in terms of an apparent H<sup>+</sup>-diffusion coefficient,  $D_{\text{H}}^{\text{app}}$ .

The validity of the two protocols was explored using a mathematical model, as shown in Fig. 3. In panel A, repetitive H<sub>i</sub><sup>+</sup>-uncaging at 0.11 Hz (Protocol 1) was simulated at the left end of a rectangular model-cell. For a given value of  $D_{\text{H}}^{\text{app}}$ , this produces local stepwise increments in [H<sup>+</sup>]<sub>i</sub>, which start to dissipate into neighboring regions. The result is a saw-toothed rise of [H<sup>+</sup>]<sub>i</sub> averaged within an ROI positioned over the H<sup>+</sup>-uncaging region. The time course, however, becomes smoother the more distal the ROI is positioned from the release site. In actual experiments, data acquisition would normally take place at the midpoint between flash-events, as indicated by the solid circles. These points are readily fitted by a two-dimensional diffusion equation (*dashed lines*), taking the same value for  $D_{\text{H}}^{\text{app}}$ , but assuming a constant localized source of acid-injection at the release-site. We therefore used the simpler, constant-source model (16) when analyzing experimental data obtained with repetitive quantal uncaging.

Fig. 3 *B* illustrates the results of modeling a brief burst of six flash-events and the subsequent relaxation of the pH<sub>i</sub> nonuniformity (Protocol 2). The solid symbols represent pH<sub>i</sub> at intervals, equivalent to the pH-sampling periods used during experiments (2.1 s), whereas the continuous lines are the full time courses predicted by the model. The relaxation



**FIGURE 3** Protocols for producing localized acid-loads. A computational model was used to simulate localized H<sup>+</sup>-uncaging within a rectangular model-cell (100 × 25 μm) featuring a  $D_{\text{H}}^{\text{app}}$  of 10<sup>-6</sup> cm<sup>2</sup>/s. (A) Protocol 1: simulation of repetitive H<sup>+</sup>-uncaging at 0.11 Hz (denoted by arrows) in a small ROI (5 × 5 μm) positioned at the left end of the cell (see schematic diagram at top). The [H<sup>+</sup>]<sub>i</sub>-rise averaged in three downstream 15 × 15 μm ROIs is plotted versus time. Solid circles denote the mid-times between flash-events. The dashed lines illustrate the solution to a constant-source diffusion equation. (B) Protocol 2: simulation of brief sequence of flash-events in a 10 × 10 μm ROI positioned at the left end of the model-cell (*inset*). After inducing a 150 nM longitudinal H<sup>+</sup>-gradient, flash-

ing was stopped to allow the gradient to relax. Time courses of the rise and subsequent relaxation of [H<sup>+</sup>]<sub>i</sub> in three downstream 15 × 15 μm ROIs are plotted as the continuous curves. Solid symbols indicate the expected timing of pH<sub>i</sub> data acquisition during the relaxation phase.

phase can be simulated using a two-dimensional diffusion equation in a closed compartment, featuring a nonuniform initial condition given by the longitudinal  $\text{pH}_i$ -profile predicted after the final flash-event.

### Local $\text{H}^+$ -uncaging in isolated myocytes

The two acid-loading protocols were applied in experiments on rat myocytes superfused with HEPES-buffered NT containing  $30\ \mu\text{M}$  cariporide. The myocyte illustrated schematically in Fig. 4 *Ai* was exposed at 0.11 Hz to flash-events over a small  $5 \times 5\ \mu\text{m}$  ROI set toward the left end of the cell (Protocol 1). Spatial  $\text{pH}_i$  data were acquired midway between flash-events, and these data points were interpolated to obtain  $[\text{H}^+]_i$  time courses in three ROIs, as shown in Fig. 4 *Ai*. The delay of  $\sim 25\ \text{s}$  between acidification in the proximal (red) and distal (blue) ROIs reflects a low mean value of  $D_{\text{H}}^{\text{app}}$ , estimated to be  $10 \times 10^{-7}\ \text{cm}^2/\text{s}$  in that particular cell (curve best-fit to data is plotted in black, Fig. 4 *Ai*). The goodness-of-fit between the model and experimental data was confirmed by plotting the measured longitudinal elevation of  $[\text{H}^+]_i$  along a cell-wide ROI at different times after commencing the flash-sequence (Fig. 4 *Aii*), and superimposing this with model-predictions using the same mean value of  $D_{\text{H}}^{\text{app}}$  (black lines, Fig. 4 *Aii*).

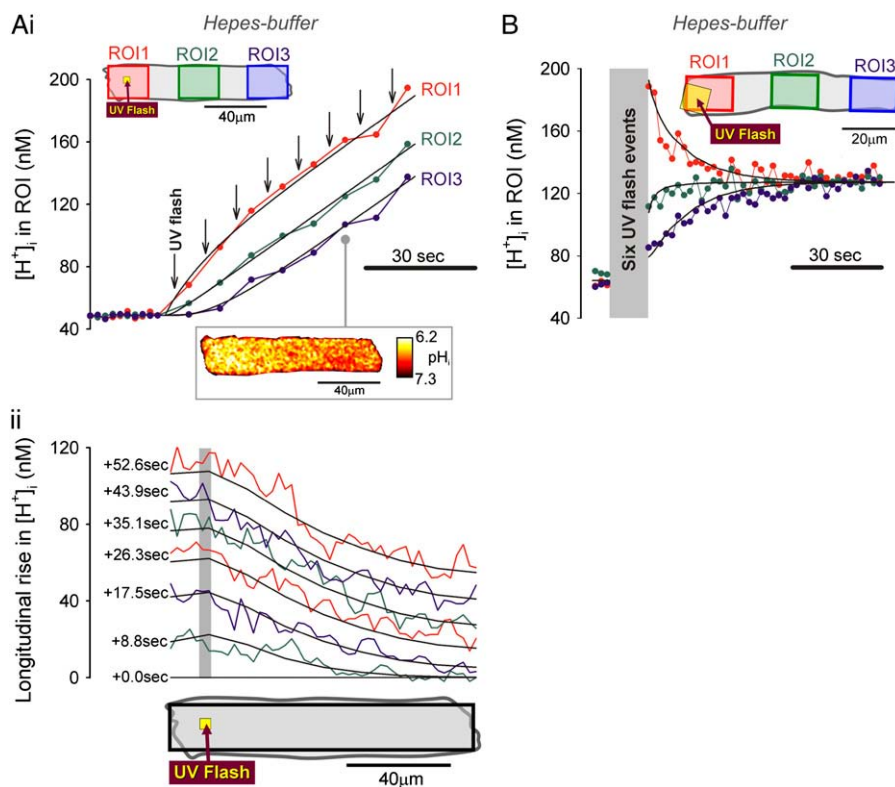
In a different myocyte, a  $10 \times 10\ \mu\text{m}$  ROI was exposed to a burst of six flash-events within a period of 12 s (Protocol 2), giving rise to an acute longitudinal  $\text{pH}_i$  nonuniformity. After the brief burst, the subsequent dissipation of the  $\text{pH}_i$

gradient is illustrated by the convergence of  $[\text{H}^+]_i$  time courses measured in three ROIs (Fig. 4 *B*). When best-fitted with a diffusion equation, these data yielded a  $D_{\text{H}}^{\text{app}}$  of  $5.5 \times 10^{-7}\ \text{cm}^2/\text{s}$ .

The spatiotemporal behavior of  $\text{H}_i^+$  in the sample experiments illustrated in Fig. 4 is consistent with that observed previously using a different technique where  $\text{H}^+$ -ions were introduced locally into a ventricular myocyte through a cell-attached micropipette. It is indicative of a diffusive process. The values derived for  $D_{\text{H}}^{\text{app}}$  are also within the range of previous estimates, suggesting that  $\text{H}_i^+$ -uncaging is a viable approach for investigating  $\text{H}_i^+$ -mobility. Results derived for  $D_{\text{H}}^{\text{app}}$  will be analyzed in more detail in a later section.

### Local $\text{H}^+$ -uncaging in myocyte cell-pairs

Photolytic uncaging of acid need not be limited to single cells. Fig. 5 illustrates the results of an experiment performed on a rat ventricular cell-pair superfused with HEPES-buffered NT containing  $30\ \mu\text{M}$  cariporide. A  $5 \times 5\ \mu\text{m}$  region at the left end of one of the cells of the pair was exposed repetitively to flash-events (Protocol 1). As expected, the localized acid-load spread rightward along the proximal cell and permeated into the second cell across the gap junctional region (Fig. 5 *Ai*). This phenomenon has been demonstrated previously while using a micropipette to load acid directly into one cell of the pair (20). When the longitudinal elevation in  $[\text{H}^+]_i$  was measured at different times



**FIGURE 4** Local  $\text{H}^+$ -uncaging in an isolated myocyte (*Ai*). Protocol 1: rat myocyte, superfused with HEPES-buffered Tyrode containing 1 mM NBA and  $30\ \mu\text{M}$  cariporide. Repetitive flash-events (0.11 Hz) were applied to a  $5 \times 5\ \mu\text{m}$  ROI positioned at the left end of the cell.  $[\text{H}^+]_i$  was averaged in three ROIs every 2.1 s (colored circles, coded to match the colored ROIs shown in schematic diagram at top); points have been interpolated to form continuous time courses. Superimposed black traces show best-fit solutions to a constant-source diffusion equation with a  $D_{\text{H}}^{\text{app}}$  of  $10 \times 10^{-7}\ \text{cm}^2/\text{s}$ . Inset shows a calibrated pH-map during acid-loading, taken at the time indicated. (*Aii*) Data from (*i*) are presented (colored traces) as longitudinal  $[\text{H}^+]_i$ -profiles at consecutive times, together with best-fit model predictions (black lines). The shaded vertical bar indicates the position of the  $\text{H}^+$ -uncaging site. (*B*) Protocol 2: rat myocyte, superfused with HEPES-buffered Tyrode containing 1 mM NBA and  $30\ \mu\text{M}$  cariporide. Six UV flash-events (0.5 Hz) were applied to a  $15 \times 15\ \mu\text{m}$  ROI positioned toward the left end of the cell. After termination of flash sequence, the relaxation of  $[\text{H}^+]_i$  averaged in three ROIs (traces color-coded to match ROIs shown in schematic diagram) is shown, along with superimposed best-fit model-predictions (black traces) for a  $D_{\text{H}}^{\text{app}}$  of  $5.5 \times 10^{-7}\ \text{cm}^2/\text{s}$ .



before and after commencement of the flash sequence, a large [H<sup>+</sup>]<sub>i</sub>-discontinuity was evident across the junction (Fig. 5 A*ii*), demonstrating that this region is rate-limiting for cell-to-cell H<sup>+</sup>-ion transmission (20,31). Using a coupled two-compartment diffusive model with a constant local source for H<sup>+</sup>-ions, and assuming H<sup>+</sup>-ion reflection at all but the junctional boundaries, the data in Fig. 5 A were deconvoluted to give an estimate of the apparent proton permeability constant ( $P_H^{\text{app}}$ ) across the junction. Fig. 5 B pools results for  $P_H^{\text{app}}$  from several H<sup>+</sup>-uncaging experiments performed on myocyte cell-pairs. The mean  $P_H^{\text{app}}$  evaluated with this technique,  $3.60(\pm 1.07) \times 10^{-4}$  cm/s, is similar to previous estimates of  $2.03(\pm 0.66) \times 10^{-4}$  cm/s and  $4.45(\pm 0.21) \times 10^{-4}$  cm/s measured using micropipette H<sup>+</sup>-injection (20) or local weak acid/base microperfusion techniques (31). The presence of the gap junctional inhibitor,  $\alpha$ -glycyrrhetinic acid ( $\alpha$ GA) at 60  $\mu$ M reduced  $P_H^{\text{app}}$  by 70–80% (Fig. 5 B), consistent with inhibition of H<sup>+</sup>-passage through ventricular connexin channels (20).

Results of local H<sub>i</sub><sup>+</sup>-uncaging in ventricular cell-pairs are thus comparable with those seen using other, more conventional acid-loading techniques (20,31). We conclude that H<sup>+</sup>-uncaging from NBA is suitable for estimating cell-to-cell H<sup>+</sup>-permeability as well as cytoplasmic H<sup>+</sup>-mobility. We also conclude that inclusion of 1 mM NBA within

cardiac myocytes does not influence the spatial movement of H<sup>+</sup> within the cell or its permeation through connexin channels.

### pH<sub>i</sub>-dependence of intracellular H<sup>+</sup>-ion mobility

To resolve the pH<sub>i</sub>-dependence of H<sup>+</sup>-ion mobility, starting pH<sub>i</sub> was manipulated uniformly to different levels before locally uncaging H<sup>+</sup> from NBA. Manipulation was achieved by prepulsing the cell with solutions containing the salt of a membrane-permeant weak acid (e.g., sodium acetate) or weak base (e.g., ammonium chloride), as described in the Methods section. On returning to normal Tyrode, pH<sub>i</sub> respectively alkalized and acidified (25). The pH<sub>i</sub> was then stabilized at the new level by inhibiting sarcolemmal H<sup>+</sup>-equivalent transport (see Methods).

H<sub>i</sub><sup>+</sup>-uncaging experiments were repeated over a range of starting pH<sub>i</sub>-values in the presence and absence of extrinsic carbonic buffer. Cumulative acid-loading (Protocol 1) in the presence of carbonic buffer is illustrated in Fig. 6 A. As with HEPES-buffer, [H<sup>+</sup>]<sub>i</sub> increased fastest close to the site of H<sup>+</sup>-release, whereas it rose more slowly in downstream regions. The estimated  $D_H^{\text{app}}$  for the cell shown in Fig. 6 A was  $22 \times 10^{-7}$  cm<sup>2</sup>/s and was higher than that typically measured for cells superfused with HEPES-buffer.

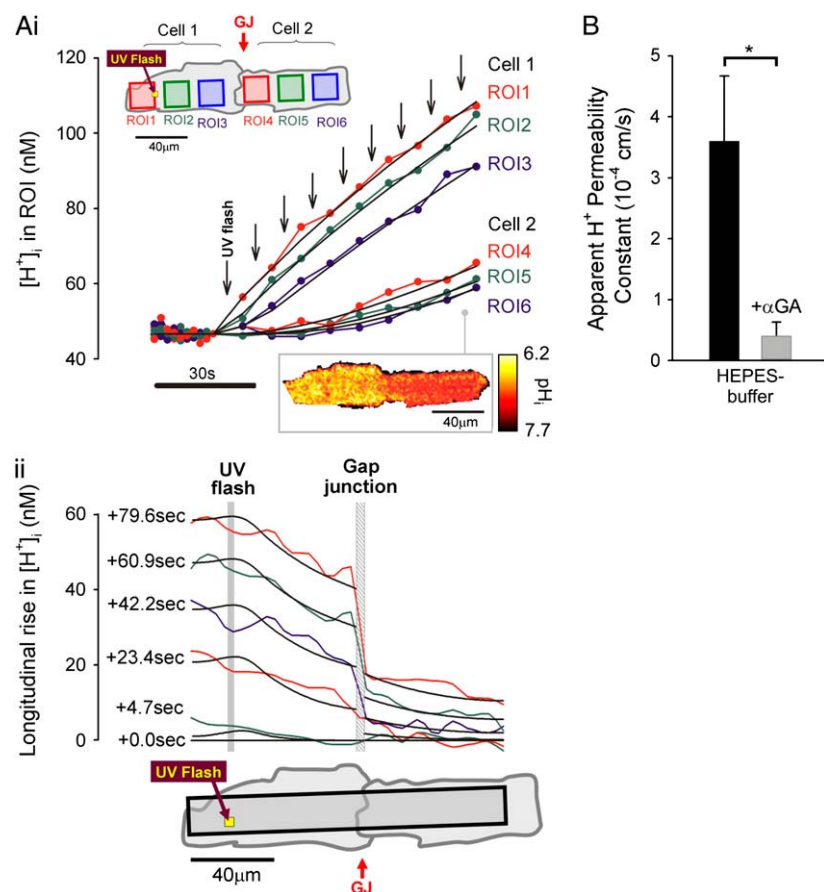


FIGURE 5 Local H<sup>+</sup>-uncaging in a myocyte cell-pair (A*i*). End-to-end rat myocyte cell-pair, superfused with HEPES-buffered Tyrode containing 1 mM NBA and 30  $\mu$ M cariporide. Repetitive flash-events (0.11 Hz) were applied to a  $5 \times 5$   $\mu$ m ROI at the left end of the cell-pair. The color-coded time courses illustrate the cumulative rise in [H<sup>+</sup>]<sub>i</sub>. The superimposed black traces show best-fit solutions to a constant-source diffusion equation with a  $D_H^{\text{app}}$  of  $9.5 \times 10^{-7}$  cm<sup>2</sup>/s and a  $P_H^{\text{app}}$  of  $1.6 \times 10^{-3}$  cm/s. Inset shows a calibrated pH-map during acid loading, taken at the time indicated. (A*ii*) Data from *i* are presented as longitudinal [H<sup>+</sup>]<sub>i</sub>-profiles at consecutive times, together with best-fit model-predictions. The vertical solid-gray bar indicates position of the acid-release site; diagonally lined bar highlights a discontinuity in the [H<sup>+</sup>]<sub>i</sub>-profile coincident with the gap junction. (B) Mean  $\pm$  SE for  $P_H^{\text{app}}$  measured with ( $n = 6$ ) and without ( $n = 7$ ) 60  $\mu$ M  $\alpha$ -glycyrrhetinic acid ( $\alpha$ GA) in superfusates, derived from experiments like that shown in A*i*. Asterisk denotes significant difference ( $P < 0.05$ ).

Values of  $D_{\text{H}}^{\text{app}}$  are plotted in Fig. 6 B versus the cell-averaged  $\text{pH}_i$  measured during the cumulative acid-load (see Methods). Values derived from cumulative  $\text{H}_i^+$ -loading (Protocol 1; red, blue triangles) as well as post-loading  $\text{H}_i^+$ -relaxation (Protocol 2; open squares) have been included. In some  $\text{H}^+$ -loading experiments performed in the presence of  $\text{CO}_2/\text{HCO}_3^-$  buffer (green triangles), 100  $\mu\text{M}$  acetazolamide (ATZ) was added to superfusates, to retard carbonic buffer equilibration. This is normally catalyzed by endogenous carbonic anhydrase (CA) (32–34).

The data pooled in Fig. 6 B show that, for experiments performed under HEPES-buffered conditions,  $D_{\text{H}}^{\text{app}}$  decreases by about sixfold as mean  $\text{pH}_i$  decreases from 7.5 to 6.1. Results from the two acid-loading protocols were very similar when compared over a common  $\text{pH}_i$ -range. The relationship between  $\text{pH}_i$  and intrinsic  $D_{\text{H}}^{\text{app}}$  is similar to that deduced previously in rat and guinea pig ventricular myocytes (dashed line) using a dual microperfusion technique (12).

$D_{\text{H}}^{\text{app}}$  in the presence of  $\text{CO}_2/\text{bicarbonate}$ -buffer was consistently higher than in HEPES, but its value still declined with  $\text{pH}_i$  (Fig. 6 B). Fig. 6 C plots the carbonic-induced increment of  $D_{\text{H}}^{\text{app}}$  over the whole  $\text{pH}_i$  range tested. It is largest at  $\sim 7.5$  and decreases monotonically as  $\text{pH}_i$  falls. Interestingly, the decline is similar to that for intrinsic  $\text{H}^+$ -

mobility. This is confirmed in Fig. 6 D which plots the fraction of  $D_{\text{H}}^{\text{app}}$  attributable to carbonic buffer alone. This fraction remains close to 30% over the  $\text{pH}_i$  range. Thus the  $\text{pH}_i$ -dependent properties of intrinsic and extrinsic  $\text{H}_i^+$ -mobility show virtually identical  $\text{pH}_i$ -sensitivity, resulting in near constant fractional contributions to  $\text{H}_i^+$ -mobility as  $\text{pH}_i$  is varied. The extrinsic component appeared to be dependent upon CA activity, as it was abolished by ATZ, leaving only the intrinsic component of  $D_{\text{H}}^{\text{app}}$ .

## DISCUSSION

### $\text{H}_i^+$ -uncaging reveals pH-sensitivity of $\text{H}_i^+$ -mobility

Photolytic uncaging of  $\text{H}^+$ -ions from intracellular NBA provides a unique way of examining  $\text{H}^+$ -ion dynamics in the cardiac ventricular myocyte. The technique has allowed us to assess the relative roles of intrinsic (non- $\text{CO}_2$ ) and extrinsic (carbonic) buffer, in the regulation of  $\text{H}_i^+$ -mobility. We find that the ability of both types of buffer to mediate intracellular  $\text{H}^+$ -ion movement declines about sixfold as intracellular pH decreases from 7.5 to 6.1. As  $\text{pH}_i$  falls, carbonic buffer's fractional contribution to  $D_{\text{H}}^{\text{app}}$  remains constant, at  $\sim 30\%$ . A

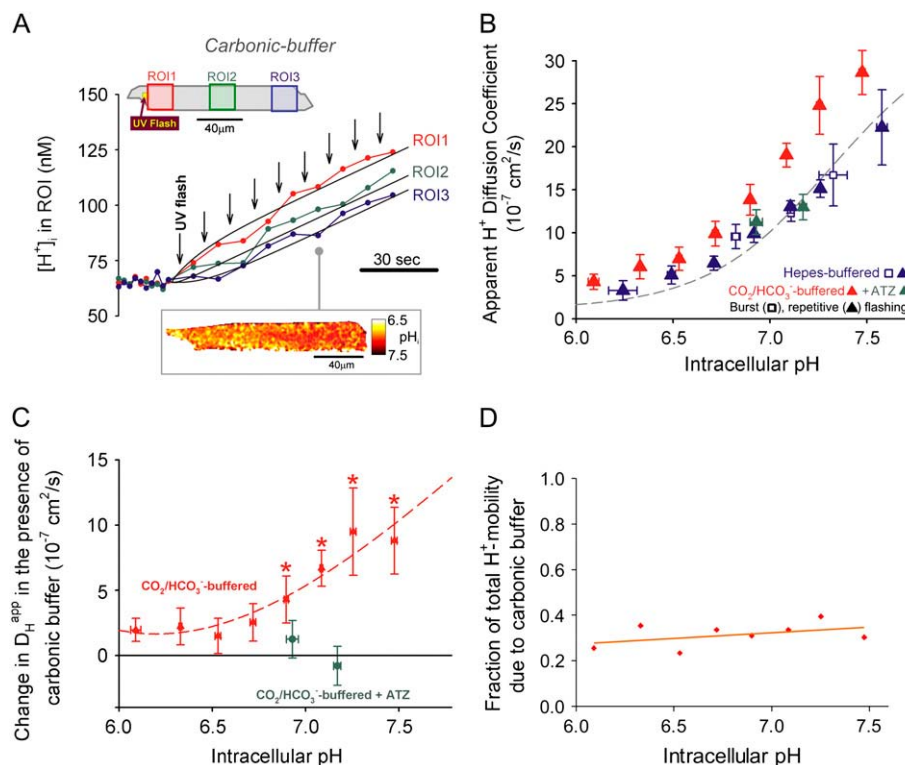


FIGURE 6 Intrinsic and extrinsic components of  $\text{H}_i^+$ -mobility are both pH-sensitive (A). A rat myocyte was superfused with  $\text{CO}_2/\text{HCO}_3^-$ -buffered Tyrode containing 1 mM NBA and 30  $\mu\text{M}$  cariporide. Repetitive flash-events (0.11 Hz) were applied to a  $5 \times 5 \mu\text{m}$  ROI positioned at the left end of the cell (protocol 1). The colored circles show the rise of  $[\text{H}^+]$  averaged in three ROIs (color-coded as shown in schematic diagram at top). Superimposed black traces show best-fit solutions to a constant-source diffusion equation with a  $D_{\text{H}}^{\text{app}}$  of  $22 \times 10^{-7} \text{ cm}^2/\text{s}$ . Inset at bottom shows a calibrated pH-map of the cell during acid-loading, taken at time indicated. (B) Experiments using either protocol 1 (solid triangles) or 2 (open squares) for local  $\text{H}^+$ -uncaging (see text, and Fig. 3) in an isolated myocyte were performed from a range of starting  $\text{pH}_i$ -values, while superfusing the cell with HEPES-buffered (blue symbols) or  $\text{CO}_2/\text{HCO}_3^-$ -buffered (red symbols) solution. Starting  $\text{pH}_i$  was preset using a weak acid/base prepulse technique (see Methods). Blue triangles,  $n = 4, 11, 34, 46, 98, 42, 25$ ; blue open squares,  $n = 19, 22, 5$ ; red triangles,  $n = 7, 10, 11, 10, 18, 37, 9, 8$ . The dashed line illustrates the  $\text{pH}_i$ -dependence of  $D_{\text{H}}^{\text{app}}$  measured previously using a different technique

(12). All red data-points are significantly different from the dashed line (z-test, 95% confidence level). In some experiments, 100  $\mu\text{M}$  ATZ was added to  $\text{CO}_2/\text{HCO}_3^-$  superfusates to block carbonic anhydrase (green triangles,  $n = 17, 19$ ). These data points were not significantly different from the dashed line (z-test, 95% confidence level). (C) The change in  $D_{\text{H}}^{\text{app}}$  in the presence of  $\text{CO}_2/\text{HCO}_3^-$  buffer is plotted as a function of  $\text{pH}_i$  (red symbols, without ATZ; green symbols, with ATZ). The dashed red line represents the difference between the best-fit sigmoidal curve to the  $D_{\text{H}}^{\text{app}}$  data in the presence and absence of carbonic buffer. (D) The fraction of  $D_{\text{H}}^{\text{app}}$  that is measured in  $\text{CO}_2/\text{HCO}_3^-$ -buffered solution (in the absence of ATZ) that is attributable to carbonic (i.e., nonintrinsic) buffering. This fraction is close to 0.3 over the entire  $\text{pH}_i$ -range studied. Data points in panels B and C show mean  $\pm$  SE.



comparable p*H*<sub>i</sub>-sensitivity of intrinsic  $D_{\text{H}}^{\text{app}}$  has been reported previously for rat and guinea pig myocytes (12), using a radically different technique (local p*H*<sub>i</sub>-displacement with membrane-permeant weak acid or base). In that work, however, experiments were not performed in the presence of carbonic buffer so the p*H*<sub>i</sub>-sensitivity of extrinsic H<sub>i</sub><sup>+</sup>-mobility could not be explored.

The physiological benefit of a decline in  $D_{\text{H}}^{\text{app}}$  with p*H*<sub>i</sub> is unclear, but it may represent a strategy for slowing the spatial spread of a local intracellular acid insult, both within a cell and within a multicellular region. Intracellular acid-overload is potentially damaging to cardiac tissue, as it is associated with intracellular Ca<sup>2+</sup>-overload (35,36), leading to electrical and mechanical malfunction (6,8,9). Slow spatial spread of H<sup>+</sup>-ions may, for example, facilitate their local removal via sarcolemmal transport mechanisms, thus restricting their global impact on the myocardium.

The p*H*<sub>i</sub>-dependence of  $D_{\text{H}}^{\text{app}}$  revealed using H<sup>+</sup>-uncaging, indicates that in the presence of CO<sub>2</sub>/HCO<sub>3</sub><sup>−</sup>, total  $D_{\text{H}}^{\text{app}}$  at p*H*<sub>i</sub> 6.1 is  $\sim 4 \times 10^{-7}$  cm<sup>2</sup>/s. This value is nearly 300-fold lower than H<sup>+</sup>-mobility in water (at 37°C,  $D_{\text{H}} = 12 \times 10^{-5}$  cm<sup>2</sup>/s). Such low mobility predicts that acidosis will predispose intracellular pH to spatial non-uniformity. Indeed such non-uniformity at low p*H*<sub>i</sub> has already been observed in the ventricular myocyte during stimulation of sarcolemmal Na<sup>+</sup>-H<sup>+</sup> exchange (13). Intracellular pH nonuniformity induced by stimulation of H<sup>+</sup>-equivalent membrane transport has also been observed in epithelial cells (15), and in invertebrate and mammalian neurons (37,38). It seems likely that, in these cell-types, a similar decline of H<sub>i</sub><sup>+</sup>-mobility with p*H*<sub>i</sub> will contribute to the generation of local p*H*<sub>i</sub> microdomains.

### Flash-photolysis of NBA: a novel experimental tool

NBA appears suitable for intracellular proton uncaging. In the mammalian ventricular myocyte, its toxicity is minimal at the doses used. In the absence of UV flashing, 1 mM NBA had no effect on diastolic Ca<sub>i</sub><sup>2+</sup> or on the time course and amplitude of an electrically-evoked Ca<sup>2+</sup>-transient. It also had no direct effect on cellular contraction, although an unexplained slowing of the later stage of relaxation was sometimes detected. Most importantly, 1 mM NBA had no effect on the mechanisms of spatial p*H*<sub>i</sub> regulation, as evidenced by a lack of effect on estimates of H<sub>i</sub><sup>+</sup>-mobility ( $D_{\text{H}}^{\text{app}}$ ) and cell-to-cell H<sup>+</sup>-permeability ( $P_{\text{H}}^{\text{app}}$ ). Flash-photolysis of intracellular NBA should therefore be an important new tool in the study of p*H*<sub>i</sub> regulation.

### Advantages of the technique

The technique can be used to produce whole-cell as well as local p*H*<sub>i</sub>-changes (cf. Fig. 2 with 4). Experiments need not be limited to single-cells but can be performed equally well on cell-pairs, and may also be suitable for tissue or whole-organ studies. UV flashing in the absence of NBA had no effect on

p*H*<sub>i</sub> (Fig. 2 *D*), eliminating the possibility of an acid-source other than NBA, or of an artifactual UV-interaction with intracellular carboxy-SNARF. We assessed the technique as an alternative to previous approaches for inducing p*H*<sub>i</sub> nonuniformity. These have comprised localized myocyte-exposure to weak acids or bases (17,18,31) or localized acid-loading via a patch pipette (11,14,16,20). UV flash-photolysis of caged-H<sup>+</sup> compounds was a simpler technique to use, with a much higher success rate experimentally. Furthermore, unlike the other two acid-loading techniques, the size, speed, and magnitude of intracellular loading could readily be varied during an experiment by adjusting the UV laser intensity.

Intracellular NBA photolysis has previously been tested in snail neurons (19) but the physicochemical properties of the technique were not quantified. In this work we monitored p*H*<sub>i</sub> ratiometrically and estimated the magnitude of local and whole-cell p*H*<sub>i</sub>-changes. When exposed to a dose of UV light, NBA releases a quantity of acid (Fig. 2 *C*) that is dependent on the laser intensity (Fig. 2 *E*). At 100% laser intensity (20 mW) the photolytic efficiency is very high, reaching 80% (i.e., during a single flash, 0.80 mM acid was released per 1 mM NBA). This is a considerably higher efficiency than that attained with other caged-H<sup>+</sup> compounds such as 4-formyl-6-methoxy-3-nitrophenoxycetic acid (39).

Since 2-nitrosobenzoic acid, the product of NBA photolysis, has a low p*K*, it will fully dissociate into H<sup>+</sup> and 2-nitrosobenzoate in the physiological pH range and produce an acid-load that is independent of p*H*<sub>i</sub>. H<sup>+</sup>-ions are therefore trapped intracellularly, and the trapping becomes cumulative during a series of flash-events (Fig. 3). In this respect, NBA is better than a substance such as 2-hydroxyphenyl 1-(2-nitrophenyl)ethyl phosphate (40) which has a p*K* value near 5, and therefore does not fully dissociate, so that its acid-delivery will vary with p*H*<sub>i</sub>. Its anionic conjugate-base will also contribute to cytoplasmic H<sup>+</sup>-buffering capacity.

Owing to the high membrane-permeability of NBA, its inclusion in the superfusate effectively clamps its intracellular concentration. The compound is also rapidly replenished after photolysis and was never a limiting factor in this work (cf. the linearity of the relationship shown in Fig. 2 *E* between the concentration of acid uncaged and that of NBA). Some previously used H<sup>+</sup>-donors, e.g., 4-formyl-6-methoxy-3-nitrophenoxycetic acid (39) are poorly membrane-permeant and therefore less suitable.

### Disadvantages of the technique

These are fourfold. Firstly, as alluded to above, prolonged exposure to intense UV light causes cell damage, but we have defined experimental protocols that appear to minimize this. Secondly, NBA appeared to be cytotoxic at concentrations as high as 10 mM, although such effects were minimal at 1 mM. We have not specifically examined the nature of NBA-toxicity but, at high concentration, NBA has tissue-fixative properties. In view of this, it may be prudent to limit

its dosage to no more than 1 mM. Thirdly, photolysis of NBA will cause intracellular accumulation of nitrosobenzoate and, at high concentration, this will impose an untoward osmotic stress on the cell. For modest whole-cell acid-loads or for spatially localized uncaging maneuvers, this is unlikely to present a serious problem. For example, a whole cell acid-load of 0.5 pH<sub>i</sub> units would release ~25 mM nitrosobenzoate, causing an increase of intracellular osmolarity of ~8%, which will induce osmotic swelling. This level of osmotic loading is well tolerated by cardiac myocytes. Indeed acid-loading by any experimental technique, or indeed metabolically by the cell itself, is likely to be accompanied by a comparable osmotic load, as protons must be added with an equivalent anionic charge, much of which will be osmotically active. The fact, however, that nitrosobenzoate is membrane impermeant, and therefore cannot escape from the cell, should be borne in mind when contemplating prolonged NBA-uncaging experiments. Fourthly, because it is so membrane permeant, NBA may well gain access to intracellular organelles. The uncaging procedure may therefore release H<sup>+</sup>-ions directly into the sarcoplasmic reticulum or into mitochondria, in addition to the cytoplasm. In our present single-photon excitation system, this effect may be amplified by photolytic H<sup>+</sup>-release within the cones of UV illumination above and below the confocal plane (this latter problem would be greatly reduced by multiphoton excitation exclusively in the confocal plane). Where H<sup>+</sup>-ion release into organelles is considered to be a potential problem, it may be prudent to compare results with those obtained using a cell-attached acid-filled micropipette (where H<sup>+</sup>-ions initially access only the cytoplasm). In the present determinations of intrinsic  $D_{\text{H}}^{\text{app}}$ , for example, it is unlikely that possible H<sup>+</sup>-release into organelles was significantly interfering with measurements of cytoplasmic H<sup>+</sup>-movement, as  $D_{\text{H}}^{\text{app}}$  was comparable when measured by both techniques. Overall, when reviewing the use of intracellular NBA as an experimental tool it would seem that, for many experimental purposes, the advantages far outweigh the disadvantages.

## MECHANISM OF pH-SENSITIVE H<sub>i</sub><sup>+</sup>-MOBILITY

### Intrinsic H<sub>i</sub><sup>+</sup>-mobility

We have shown previously that the pH<sub>i</sub>-dependence of intrinsic  $D_{\text{H}}^{\text{app}}$  is consistent with two pooled populations of intrinsic buffer (12). One appears to have very low or zero mobility, most likely represented by buffer sites on intracellular proteins. The other appears to be more mobile, represented by lower molecular weight molecules such as the histidyl dipeptides (100–200 Da) that are prevalent in many tissues, including heart (41) and skeletal muscle (42). As described in the Introduction, H<sub>i</sub><sup>+</sup>-mobility is dependent on spatial H<sup>+</sup>-shuttling by these mobile buffer molecules. They are estimated to have a pooled diffusion coefficient,  $D_{\text{mob}}$ , equal to  $49.9 \times 10^{-7} \text{ cm}^2/\text{s}$  (12). Since the intrinsic buffers

equilibrate rapidly (25), the apparent diffusion coefficient ( $D_{\text{H}}^{\text{app}}$ ) can be described using the equation:

$$D_{\text{H}}^{\text{app}} = \frac{D_{\text{mob}} \times \beta_{\text{mob}}}{\beta_{\text{mob}} + \beta_{\text{fix}}}, \quad (1)$$

where  $D_{\text{mob}}$  and  $\beta_{\text{mob}}$  denote the intrinsic mobile buffer diffusion coefficient and capacity respectively, and where  $\beta_{\text{fix}}$  denotes the intrinsic fixed buffer capacity (11,43). On this scheme, the pH<sub>i</sub>-dependence of intrinsic  $D_{\text{H}}^{\text{app}}$  is consistent with a pH<sub>i</sub>-dependence of  $\beta_{\text{mob}}$  and  $\beta_{\text{fix}}$ , the former having a mean pK of ~7.48 and the latter a much lower mean pK of 6.40 (12). Thus as pH<sub>i</sub> decreases from a resting value of ~7.1,  $\beta_{\text{mob}}$  also decreases as it becomes saturated with H<sup>+</sup>-ions, whereas  $\beta_{\text{fix}}$  increases as ambient pH approaches its pK. The mobile fraction of intrinsic buffering thus decreases, resulting in a fall of H<sub>i</sub><sup>+</sup>-mobility.

### Extrinsic H<sub>i</sub><sup>+</sup>-mobility

#### Comparison with previous work

Introducing carbonic buffer into a rat myocyte increased  $D_{\text{H}}^{\text{app}}$  by ~50% (i.e., the extrinsic component of  $D_{\text{H}}^{\text{app}}$  is ~30% of total  $D_{\text{H}}^{\text{app}}$ ). Although an increase was found in previous work on guinea-pig and rabbit ventricular myocytes, it appeared to be much larger (two- to fivefold). Some of this discrepancy may represent species differences, but there are other possible explanations. Firstly, initial work with CO<sub>2</sub>/HCO<sub>3</sub><sup>−</sup> buffer (14) estimated  $D_{\text{H}}^{\text{app}}$  from the time delay for H<sup>+</sup>-ion diffusion down a cell, when injected locally from a micropipette. Unlike more recent analyses (16,29), the specific geometry of each cell was not taken into account (myocyte geometry was standardized as rectangular). As a result, errors in estimating  $D_{\text{H}}^{\text{app}}$  may have arisen, particularly when the time delay was small. Secondly, most previous work did not acknowledge the pH<sub>i</sub>-dependence of  $D_{\text{H}}^{\text{app}}$ . The graph shown in Fig. 6 B illustrates that carbonic buffer's contribution is  $2 \times 10^{-7} \text{ cm}^2/\text{s}$  at pH<sub>i</sub> 6.1, rising to nearly  $10 \times 10^{-7} \text{ cm}^2/\text{s}$  at pH<sub>i</sub> 7.5. The intrinsic contribution varies from  $2.5\text{--}22 \times 10^{-7} \text{ cm}^2/\text{s}$  over the same range (Fig. 6 A), which encompasses the averaged values for intrinsic  $D_{\text{H}}^{\text{app}}$  reported previously (typically  $\sim 8 \times 10^{-7} \text{ cm}^2/\text{s}$ ). Thus, if H<sub>i</sub><sup>+</sup>-mobility values were not compared at a common pH<sub>i</sub>, the contribution of carbonic buffer would appear to range from 10% to 500%. Clearly the procedure of using a common pH<sub>i</sub> value when comparing  $D_{\text{H}}^{\text{app}}$  values must now be adopted. A final reason for differing estimates of carbonic buffer's contribution to H<sub>i</sub><sup>+</sup>-mobility may be its slow kinetics, which permit the buffer to mediate slow, but not fast, H<sub>i</sub><sup>+</sup>-shuttling reactions. We return to this point in a later section.

### Extrinsic H<sub>i</sub><sup>+</sup>-mobility constrained by fixed buffers and [HCO<sub>3</sub><sup>−</sup>]<sub>i</sub>

HCO<sub>3</sub><sup>−</sup> anions, in concert with CO<sub>2</sub>, act as mobile buffers within the cell, shuttling H<sup>+</sup>-ions spatially (14,15). Like

other mobile buffers, HCO<sub>3</sub><sup>−</sup> ions must compete with fixed intrinsic buffers for H<sup>+</sup>-ion binding. Given that β<sub>fix</sub> rises steeply as pH<sub>i</sub> falls (12,16), part of the observed decline in the effectiveness of the extrinsic shuttle at low pH<sub>i</sub> (Fig. 6 C) can be attributed to increased competition from fixed buffers. This would predict a 1.7-fold decline in extrinsic H<sup>+</sup>-mobility, rather than the fivefold decline actually observed (Fig. 6 C). Thus other factors must also play a role.

Assuming that CO<sub>2</sub> is freely permeant across the sarcolemma, so that [CO<sub>2</sub>]<sub>i</sub> is clamped by a constant extracellular [CO<sub>2</sub>], carbonic buffering capacity at equilibrium can be expressed as a function of intracellular bicarbonate concentration (24):

$$\beta_{\text{carb}} = \ln(10) \times [\text{HCO}_3^-]_i = \ln(10) \times [\text{HCO}_3^-]_o \times 10^{\text{pH}_i - \text{pH}_o}, \quad (2)$$

where subscripts *i* and *o* denote the intracellular and extracellular compartments, respectively. Equation 1 has previously been modified to describe the H<sub>i</sub><sup>+</sup>-mobility constant in the presence of carbonic buffer (14) by including two extra terms, β<sub>carb</sub> and D<sub>carb</sub> (the effective diffusion coefficient of carbonic buffer, a term lumped for the individual diffusion coefficients of intracellular CO<sub>2</sub> and HCO<sub>3</sub><sup>−</sup>, the constituents of carbonic buffer):

$$D_{\text{H}}^{\text{app}} = \frac{D_{\text{mob}} \times \beta_{\text{mob}} + D_{\text{carb}} \times \beta_{\text{carb}}}{\beta_{\text{mob}} + \beta_{\text{carb}} + \beta_{\text{fix}}}. \quad (3)$$

Assuming the cell remains fully open to CO<sub>2</sub>, much of the pH<sub>i</sub>-dependence of extrinsic H<sub>i</sub><sup>+</sup>-mobility can be explained by a fall in [HCO<sub>3</sub><sup>−</sup>]<sub>i</sub>, and hence a fall of β<sub>carb</sub> as pH<sub>i</sub> declines. Over the pH<sub>i</sub> range from 7.5 to 6.1, β<sub>carb</sub> at equilibrium falls 25-fold. This would be more than sufficient to account for the decline in the extrinsic component of H<sub>i</sub><sup>+</sup>-mobility (Fig. 6 C). During intracellular acidosis, H<sup>+</sup>-movement via the carbonic shuttle is therefore likely to be constrained by the H<sup>+</sup>-binding capacity of fixed buffers, and by the availability of intracellular bicarbonate.

### Extrinsic H<sub>i</sub><sup>+</sup>-mobility also constrained by slow buffer-kinetics

Although extrinsic H<sub>i</sub><sup>+</sup>-mobility will be influenced by [HCO<sub>3</sub><sup>−</sup>]<sub>i</sub>, quantifying this effect is not straightforward. Eq. 3 can be used to predict D<sub>H</sub><sup>app</sup> in the presence of carbonic buffer, provided the effective value for β<sub>carb</sub> is known. In this work, net H<sub>i</sub><sup>+</sup>-movement was observed over periods of 1–2 min. Unfortunately, on this timescale, β<sub>carb</sub> cannot reliably be estimated from Eq. 2, as the CO<sub>2</sub>/HCO<sub>3</sub><sup>−</sup> buffer system may not be close to equilibrium. CO<sub>2</sub>-hydration is slow and only moderately accelerated in cardiomyocytes by endogenous CA (34). As a result, intracellular carbonic buffering is also slow, often taking minutes to equilibrate. During this period, the effective value of β<sub>carb</sub> may be significantly less than its equilibrium value. This raises difficulties for computing D<sub>H</sub><sup>app</sup>.

By assigning a value to D<sub>carb</sub>, Eq. 3 can be used to explore the effective value of β<sub>carb</sub> during spatial H<sub>i</sub><sup>+</sup>-movement. After correcting for temperature and macromolecular crowding in the cytosolic environment, the intracellular diffusion coefficients for CO<sub>2</sub> and HCO<sub>3</sub><sup>−</sup> (the constituents of carbonic buffer) have been estimated as 11 and 7.7 × 10<sup>−6</sup> cm<sup>2</sup>/s, respectively (29). D<sub>carb</sub> can be represented by the lower of the two coefficients, i.e., 7.7 × 10<sup>−6</sup> cm<sup>2</sup>/s. Best-fitting the data in Fig. 6 B with Eq. 3 yields estimates for β<sub>carb</sub>, which rise from around 1 mM at pH 6.1 to 4 mM at pH 7.5. These are considerably smaller than the equilibrium values predicted from Eq. 2 (2.5 and 63 mM, respectively). The low effective values for β<sub>carb</sub> are therefore suggestive of an out-of-equilibrium state, whereby carbonic buffer contributes only a fraction of its full capacity to the shuttling of intracellular H<sup>+</sup>-ions. The exact value of this fraction will depend on the buffer's catalytic acceleration by CA, the magnitude of the spatial acid-flux, and movements of CO<sub>2</sub> across the sarcolemma. This conclusion is reinforced by the observation that extrinsic H<sub>i</sub><sup>+</sup>-mobility disappears entirely when CA is inhibited by acetazolamide (Fig. 6 B, *green triangles*).

The above calculations suggest that, during the intracellular acid-loading rate used in this study (~15 mM/min averaged over the cell), the effective value of β<sub>carb</sub> was reduced by 2.5–15-fold from its equilibrium value. Much larger spatial acid-fluxes (~100 mM/min) have been induced previously in experiments involving partial exposure of a myocyte to ammonium chloride (18). In those experiments, the presence of carbonic buffer had virtually no effect on H<sub>i</sub><sup>+</sup>-mobility, suggesting the effective value of β<sub>carb</sub> may have fallen to near zero.

The ability of the CO<sub>2</sub>/HCO<sub>3</sub><sup>−</sup>-shuttle to mediate H<sub>i</sub><sup>+</sup>-movement in the cardiac myocyte will therefore be limited, not only by fixed buffers and the availability of intracellular bicarbonate, but also by the extrinsic buffer's slow kinetics. When spatial pH<sub>i</sub> nonuniformity is large, resulting in high intracellular H<sup>+</sup>-traffic, the buffer's fractional contribution will be reduced. The present estimate of 30% should therefore be viewed in the context of the size of the underlying spatial acid-flux. Significant differences in flux magnitude may account for reported differences in the buffer's contribution to H<sub>i</sub><sup>+</sup>-mobility (this work; (14,16,18)), and in its ability to minimize pH<sub>i</sub> nonuniformity (14–16,38).

Because of uncertainty regarding the effective value of β<sub>carb</sub> during H<sub>i</sub><sup>+</sup>-shuttling, the mechanism for pH-dependent extrinsic H<sub>i</sub><sup>+</sup>-mobility has yet to be modeled quantitatively. Even if carbonic buffer is significantly out-of-equilibrium, as seems likely during some local H<sub>i</sub><sup>+</sup>-movement, the restricted availability of intracellular HCO<sub>3</sub><sup>−</sup> during acidosis will be an important constraining factor. An additional factor may be a pH<sub>i</sub>-sensitivity of the CA enzyme, as this regulates the speed of buffer equilibration (32,34). CA isoforms I and II are known to be pH-sensitive (44), but the isoforms responsible for facilitating intracellular H<sup>+</sup>-ion movement in the cardiac myocyte have yet to be identified.

## CONCLUSIONS

Flash-photolysis of intracellular NBA provides a convenient and novel tool for displacing intracellular pH. The approach is simple to implement and need not be restricted to single-cell preparations. It should prove useful in cell-types less amenable to conventional methods of local acid-injection. Using the method, we have demonstrated that, in ventricular cells, both extrinsic (carbonic) and intrinsic buffers regulate intracellular  $H^+$ -ion movement. With these experimental protocols, extrinsic buffer accounts for ~30% of  $H_i^+$ -mobility over a wide  $pH_i$ -range. The fact that this component relies upon the activity of CA indicates the important role of this enzyme in spatial  $pH_i$  regulation. The remaining 70% of  $H_i^+$ -movement is mediated by intrinsic mobile buffers. A key finding is that both extrinsic and intrinsic  $H_i^+$ -mobility are severely reduced during intracellular acidosis. This will compromise the spatial uniformity of  $pH_i$ , particularly when sarcolemmal  $H^+$ -equivalent extruders are stimulated (13). The physiological consequences of spatial  $pH_i$  nonuniformity are only now being investigated, but they are likely to include a spatial disruption of both  $Ca_i^{2+}$ -signaling (45,46) and contraction (46). Severe intracellular acidosis in the cardiac myocyte may thus present a window of vulnerability in the spatial coordination of cell function.

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